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In modern hospitals, patients are treated using a wide array of medical devices that are increasingly interacting with each other over the network. We study the safety of a medical device system for the physiologic closed-loop control of drug infusion. The main contribution is the verification approach for the safety properties of closed-loop medical device systems. The method combines simulation-based analysis of continuous patient dynamics with model checking of a more abstract timed automata model.

For Networked Medical Systems with a Patient-in-loop, how can we guarantee open-loop safety?

1 Interoperability for Patient Safety

Built according to the Integrated Clinical Environment (ICE) architecture

2 Medical Case Study: Closed-loop PCA pump

Patient Controlled Analgesia: Common technique for delivering pain medication.

- Patient presses a button to request a dose
- Overdoses result in respiratory distress, ultimately death
- Pumps have safeguards, but overdoses can still happen
- PCA is a significant source of adverse events

3 System Architecture

Control Loop

PCA Case Study

Challenges for system verification:

- Complex interplay between the continuous patient's dynamics and the discrete nature of the controller and communication network.

4 Patient Model

$$\begin{bmatrix} \dot{C}_1 \\ \dot{C}_2 \\ \dot{C}_3 \end{bmatrix} = \underbrace{\begin{bmatrix} -(k_{12} + k_{13} + k_{10}) & k_{21} & k_{31} \\ k_{12} & -k_{12} & 0 \\ k_{13} & 0 & -k_{31} \end{bmatrix}}_A \begin{bmatrix} C_1 \\ C_2 \\ C_3 \end{bmatrix} + \underbrace{\begin{bmatrix} \frac{1}{V_1} \\ 0 \\ 0 \end{bmatrix}}_B I$$

$$dl = \underbrace{\begin{bmatrix} 1 & 0 & 0 \end{bmatrix}}_C \begin{bmatrix} C_1 \\ C_2 \\ C_3 \end{bmatrix}$$

3-compartment model

- drug concentration in blood and tissue

Modeling Patient specific behavior:

$$k_{ij} \in [\hat{k}_{ij} - \Delta k_{ij}, \hat{k}_{ij} + \Delta k_{ij}]$$

$$V_1 \in [\hat{V}_1 - \Delta V, \hat{V}_1 + \Delta V]$$

Patient Critical Regions

Patient Response to Drug

- The model allows estimation of t_{crit}
- For the patient model with fixed parameters t_{crit} determined analytically

5 UPPAAL Model

PCA Pump model

Supervisor model

Network model

Properties verified with UPPAAL

- Once SpO₂ drops below pain threshold, it eventually goes back up
 $A[]$ (samplebuffer < pain_thresh -> A <> samplebuffer >= pain_thresh)
- The pump is stopped if patient enters alarming region
 $A[]$ (samplebuffer < alarm_thresh -> A <> (PCA.Rstopped V PCA.Bstopped)
- The patient can not go into the critical region
 $A[]$ (samplebuffer >= critical)

6 Timing analysis

Key Safety Property

- Pump stops in time if total delay $\leq t_{crit}$
- For model with uncertain parameters
 - Matrices A, B, C belong to regions

$$\tilde{t}_{crit} = \frac{1}{\|\tilde{A}\|} \ln \left(\frac{\frac{|\Delta H|}{gain}}{\|\tilde{C}\| \cdot (\|\tilde{x}_0\| + \frac{\|\tilde{B}u_1\|}{\|\tilde{A}_{max}\|})} + 1 \right)$$

$$\tilde{A} = \underset{A \in \mathbb{R}\{A\}}{\text{argmax}} \|A\|, \tilde{B} = \underset{B \in \mathbb{R}\{B\}}{\text{argmax}} \|B u_1\|, \tilde{C} = \underset{C \in \mathbb{R}\{C\}}{\text{argmax}} \|C\|$$

$$A_{min} = \underset{A \in \mathbb{R}\{A\}}{\text{argmin}} \|A\|$$

UPPAAL model parameters initialized to guarantee consistency between the UPPAAL model and physical patient model

$$\left\lceil \frac{\Delta H / gain}{PCA_{rateON} - ab_{rate}} \right\rceil = \lceil \tilde{t}_{crit} \rceil \quad \text{The pump is ON}$$

$$\left\lfloor \frac{\Delta H / gain}{rate_{down}} \right\rfloor = \left\lfloor \frac{1}{\|\tilde{A}\|} \ln \left(\frac{|\Delta H| / gain}{\|\tilde{C}\| \cdot (\|\tilde{x}_0\| + \frac{\|\tilde{B}u_1\|}{\|\tilde{A}_{max}\|})} + 1 \right) \right\rfloor \quad \text{OFF}$$

7 Demo

The system have been presented at:

- Annual meeting of the American Society of Anesthesiologists in 2007 (first place in the scientific exhibits)
- 2008 HIMMS (Healthcare Information and Management Systems Society) Congress
- 2008 CIMIT Innovation Congress